Dynamic imaging of pancreatic diseases by contrast enhanced coded phase inversion harmonic ultrasonography

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Background: Coded phase inversion harmonic ultrasonography, a newly available sonographic technique, enables visualisation of slow flow in minute vessels in a real time fashion with the use of a sonographic contrast agent containing monosaccharide. Our purpose was to employ this novel technique to observe microvessels in pancreatic tumours.

Subjects and methods: Sixty five patients with suspicious pancreatic tumours received contrast enhanced coded phase inversion harmonic ultrasonography, contrast enhanced computed tomography, and endosonography. Final diagnoses based on histological findings were pancreatic ductal carcinomas in 49 patients, inflammatory pseudotumours with chronic pancreatitis in seven, and endocrine tumours in nine. For contrast enhanced coded harmonic ultrasonography, Levovist, a contrast agent, was injected intravenously as a bolus. When the first microbubble signal appeared in the pancreas, images of the ideal scanning plane were displayed in a real time continuous fashion (vessel images). Subsequently, interval delay scanning (perfusion images) was taken to demonstrate parenchymal flow. Tumour vascularity was evaluated by using the two types of imaging. Sensitivities for depicting pancreatic tumours were compared between three examinations.

Results: Contrast enhanced ultrasonography demonstrated tumour vessels in 67% of pancreatic ductal carcinomas, although most were relatively hypovascular compared with the surrounding pancreatic tissue. The vascular patterns of tumours obtained by contrast enhanced ultrasonography were closely correlated with those obtained by contrast enhanced computed tomography. Values for sensitivity in depicting pancreatic tumours of 2 cm or less in size were 68% for contrast enhanced computed tomography, 95% for endosonography, and 95% for contrast enhanced ultrasonography.

Conclusion: Contrast enhanced coded phase inversion harmonic ultrasonography successfully visualised fine vessels in pancreatic tumours and may play a pivotal role in the depiction and differential diagnosis of pancreatic tumours.
Contrast enhanced US examination

To minimise the procedural variations, contrast enhanced US was performed by the same sonographer (KM) using the same examination protocol. The technique had been established by the sonographer (KM) who had conducted contrast enhanced US in more than 1000 patients before beginning the present study. The sonographer (KM) was informed that a pancreatic mass had been suspected by other imaging modalities but was blinded to the location and findings of the tumour. Ultrasonographic equipment with a 2–4 MHz curved array wide band transducer, GE LOGIQ 9, and 700 EXPERT Series units (General Electric Medical Systems, Milwaukee, Wisconsin, USA) was used for coded phase inversion imaging.10–15 The acoustic power was set at the default setting with a mechanical index of 0.6–0.8. After detecting an abnormality such as a nodule, swelling, or stenosis of the main duct in the pancreas on fundamental B-mode US, the sonographer conducted contrast enhanced US, displaying the ideal scanning plane of the lesion. When the first microbubble signal appeared in the tumour after bolus injection of 2.5 g of Levovist (a suspension of monosaccharide microparticles, 6 ml of a 400 mg/ml concentration; Schering AG, Berlin, Germany), the patient was instructed to hold his/her breath. Images of the ideal scanning plane were displayed in real time by slightly changing the scanning plane to portray the whole area of the tumour (vessel image). In addition to real time continuous imaging of the tumour vessels, interval delay scanning was performed to demonstrate tumour parenchymal flow in the blood pool phase (perfusion image, five seconds of interval time, less than 90 seconds after injection of Levovist). The entire examination was stored in a recording system and reviewed by two readers who were absent during the US examination and completely blinded to the results of the previous investigations, including fundamental B-mode US, CT, MR, and ERCP. The reviewers assessed the vascular patterns of the tumours.

Contrast enhanced CT

Contrast enhanced two phase CT (Toshiba X-vigor, Toshiba Medical System, Japan) was imaged 30 and 180 seconds after the beginning of injection of 100 ml of contrast media (Optiray 320; Yamanouchi Pharmaceutical, Tokyo, Japan) into the antecubital vein with a 5.0 mm slice thickness. Images were reviewed by two readers who were blinded to the US and pathological findings.

Endosonography

EUS was performed by two qualified (from the Japanese Gastroenterological Endoscopic Society) endoscopists (MK, RN), using an Olympus GF-UC240P-AL5 for endoscopy and an Aloka ProSound-5500 for image analysis. EUS-FNA was performed in 34 patients. The needle for the aspiration biopsy was an Olympus NA-10J-1 or an Olympus NA-11J-KB.

Statistical analysis

Sensitivities for depicting pancreatic tumours of 2 cm or less and those of more than 2 cm in size were calculated from contrast enhanced US, contrast enhanced CT, and EUS. The χ2 test for non-parametric data was performed to compare the sensitivities for depiction of tumours between the three examinations. Scheffe’s multiple comparison test was used to compare contrast indices between the four types of contrast enhanced US classified tumours. A p value of <0.05 was considered significant.

RESULTS

Normal pancreatic tissue showed several vessels distributed homogeneously on the vessel image and a homogeneous stain on the perfusion image. On the basis of the density of vessels on the vessel image and enhancement on the perfusion image relative to the surrounding pancreatic tissue,
the image patterns of the pancreatic tumours were classified into the following four types (fig 1): type I, no vessels on the vessel image and hypovascular enhancement on the perfusion image; type II, low density of vessels on the vessel image and slight heterogeneous enhancement in the hypovascular area on the perfusion image; type III, similar density of vessels to the surrounding tissue on the vessel image and homogenous isovascular enhancement on the perfusion image; and type IV, high density of vessels on the vessel image and hypervascular enhancement on the perfusion image. The contrast indices of types I, II, III, and IV were mean 0.28 (SD 0.10), 0.64 (0.17), 1.11 (0.11), and 1.76 (0.42), respectively (fig 2). The contrast indices were significantly different among the four types. A close correlation was demonstrated between the contrast index and the image pattern (fig 2).

Fourteen of 15 tumours classified as type I were ductal carcinomas (fig 3). Only one of 15 tumours was an endocrine tumour. All 29 tumours classified as type II were ductal carcinomas. On the vessel images of type II tumours, several vessels surrounding the tumour and flowing from the peripheral part to the centre of the tumour were depicted. The perfusion images of type II tumours showed a heterogeneous network-like stain of the tumour although it appeared as a hypovascular tumour relative to the surrounding tissue (fig 4). Seven inflammatory pseudotumours caused by chronic pancreatitis showed the type III pattern in which there were no differences in the images (vessel and perfusion) between the inside and outside of the tumours (fig 5). Only one of the 49 ductal carcinomas showed the type III pattern. Seven of the 10 tumours classified as type IV were endocrine tumours (fig 6). There were rich vessels on the vessel image and remarkable enhancement on the perfusion image of the endocrine tumours (fig 6). The other three tumours classified as type IV were pancreatic carcinomas. On contrast enhanced US, tumour vessels were visualised in 33
(67%) of all pancreatic ductal carcinomas (29 type II; one type III; three type IV), and most were relatively hypovascular compared with the surrounding pancreatic tissue (type II).

### Table 1

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<tr>
<th>Imaging Modality</th>
<th>Sensitivity</th>
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<tr>
<td>Contrast enhanced CT</td>
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<tr>
<td>Fundamental B-mode US</td>
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<tr>
<td>Contrast enhanced US</td>
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</table>

Table 1 shows the sensitivities of contrast enhanced CT, fundamental B-mode US, and contrast enhanced US in depicting pancreatic tumours. Fundamental B-mode US failed to depict six tumours (five ductal carcinomas and
Contrast enhanced sonography was first reported with the use of carbon dioxide microbubbles. The technique is a non-invasive and relatively safe method for diagnosing pancreatic ductal carcinomas, with a reported sensitivity of 84% and specificity of 93% for depicting pancreatic tumours. Contrast enhanced US (CEUS) has been shown to have similar diagnostic accuracy to contrast enhanced CT (CECT) in detecting and characterising pancreatic tumours, particularly in patients with chronic pancreatitis and pancreatic ductal adenocarcinomas.

**DISCUSSION**

Contrast enhanced sonography was first reported with the use of carbon dioxide microbubbles. The technique is a sensitive and accurate tool for differentiating pancreatic ductal carcinomas from chronic pancreatitis and pancreatic endocrine tumours. However, it requires an angiographic technique that is relatively invasive because carbon dioxide microbubbles are selectively infused into the coeliac artery or superior mesenteric artery. Levovist, a sonography contrast agent that is infused intravenously, was developed concurrently and is known to be well tolerated with a fairly good safety profile. However, several limitations with microbubble agents in Doppler US studies, such as blooming artefacts, poor spatial resolution, and low sensitivity to slow flow, were inevitable. The recently introduced phase inversion (pulse inversion) harmonic US technique is a microbubble specific approach that depicts signals from microbubbles sensitively with good spatial resolution devoid of Doppler related artefacts. Furthermore, the encoding technology has made it possible to observe the flow of the bubbles in a real time fashion (vessel image). We observed tumour vessels on real time continuous imaging and tumour parenchymal flow on interval delay scanning by the use of coded phase inversion harmonic imaging. In the present study, fine vessels surrounding the tumour and flowing from the periphery to the centre of the tumour in a real time fashion were visualised in 67% of all pancreatic ductal carcinomas. This pathophysiological phenomenon of pancreatic tumours was first visualised by means of this novel technology.

It is not difficult to manipulate contrast enhanced coded phase inversion harmonic US. Reliable imaging can be obtained after conducting this examination in 10–20 cases. The sonographer (KM) in the present study had conducted contrast enhanced US in more than 1000 patients before beginning the present study. The reviewers (MK and TK) had experience of more than 300 cases of reading images of contrast enhanced US. Therefore, reliable imaging and reading were performed throughout our study. On the basis of the patterns of vessel and perfusion images of contrast enhanced US, we classified tumour vascularity into four patterns. We calculated contrast indices to confirm the reliability of the classification by the reviewers, although they were obtained only from the perfusion images. The fact that the contrast indices sequentially increased from type I to type IV supports the reliability of the classification by the reviewers. Ductal carcinoma is known to be a hypovascular tumour. The typical vascular patterns of the tumour manifest low attenuation relative to the surrounding pancreatic tissue on contrast enhanced CT which is known to be useful in diagnosing pancreatic diseases.

When type I and II tumours together are categorised as a hypovascular pattern, most ductal carcinomas in the present study were hypovascular on contrast enhanced US while the other tumours were isovascular or hypervascular. The fact that the vascular patterns of the tumours on contrast enhanced US correlated well with those on contrast enhanced CT suggests that contrast enhanced US is as reliable as contrast enhanced CT for diagnosing pancreatic tumours.

Contrast enhanced US enabled depiction of the margin of the three tumours that fundamental B-mode US failed to detect, suggesting that visualisation of vascularity may assist...
in discriminating tumours from the surrounding tissue in US examinations. In addition, contrast enhanced US depicted six tumours that contrast enhanced CT failed to depict. In particular, the sensitivity of contrast enhanced US (95%) in depicting small tumours of 2 cm or less in size was remarkably different from that of contrast enhanced CT (68%). These results indicate that contrast enhanced US may be superior to contrast enhanced CT in depicting small tumours due to higher spatial resolution. Alternatively, contrast enhanced US may more clearly discriminate blood flow in the pancreatic tumour from that in the surrounding tissue. With regard to depicting ability, contrast enhanced US was similar to EUS, which is known to be superior to any other modalities with respect to spatial resolution. 

In conclusion, this new technique made it possible to depict fine vessels surrounding the tumour and flowing to the periphery of the tumour in a real-time fashion, facilitating differential diagnosis of pancreatic tumours. To the best of our knowledge, there have been no reports that have shown the architecture of fine vessels in pancreatic cancers other than by sonography. In addition, another advantage of contrast enhanced US is that it improved the depiction of small lesions compared with fundamental B-mode US and contrast enhanced CT. Further prospective controlled studies are required where magnetic resonance imaging, EUS, and contrast enhanced harmonic US should be compared with the gold standard operation and histology.

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REFERENCES